

# Biophysical Regulation of Lipid Biosynthesis in the Plasma Membrane

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**ABSTRACT** We present a cellular model of lipid biosynthesis in the plasma membrane that couples biochemical and biophysical features of the enzymatic network of the cell-wall-less Mycoplasma *Acholeplasma laidlawii*. In particular, we formulate how the stored elastic energy of the lipid bilayer can modify the activity of curvature-sensitive enzymes through the binding of amphipathic  $\alpha$ -helices. As the binding depends on lipid composition, this results in a biophysical feedback mechanism for the regulation of the stored elastic energy. The model shows that the presence of feedback increases the robustness of the steady state of the system, in the sense that biologically inviable nonbilayer states are less likely. We also show that the biophysical and biochemical features of the network have implications as to which enzymes are most efficient at implementing the regulation. The network imposes restrictions on the steady-state balance between bilayer and nonbilayer lipids and on the concentrations of particular lipids. Finally, we consider the influence of the length of the amphipathic  $\alpha$ -helix on the efficacy of the feedback and propose experimental measurements and extensions of the modeling framework.

## INTRODUCTION

The primary function of the lipids in the plasma membrane is to form a bilayer that provides a permeability barrier between the cytoplasm and the environment. However, whereas lipids were once considered purely passive components, it is now clear that lipids play an active role in a variety of dynamic processes involving the membranes that compartmentalize the cell (1). To achieve this dual role of the membrane as a dynamic boundary and a continuous barrier, the cell must regulate the mechanical properties of the membrane and does so partly by controlling its lipid composition.

Membrane lipids are chemically diverse (2) but they can be classified into the broad categories of bilayer and nonbilayer lipids, depending on their (in)ability to self-assemble into bilayers. Bilayer formation is the result of a thermodynamic equilibrium in which the physicochemical properties of the lipids, such as the chemical structure of the headgroup and hydrocarbon chains, play a crucial role. The cell can therefore regulate the mechanical properties of the bilayer by modifying its lipid composition through lipid biosynthesis. The balance between bilayer and nonbilayer lipids in the plasma membrane has been the subject of many reviews (2–4). Experiments have shown that organisms change the lipid composition of their membranes in response to external variations in diet, pressure, and temperature (5–7; see also (18)). Moreover, many of the lipids found in biological membranes do not form bilayers under physiological conditions. Subsequent studies have confirmed that most organisms contain significant amounts of at least one nonbilayer lipid (8,9).

The underlying biophysical question is the relationship between the chemical diversity and variability of membrane lipid composition, the mechanical properties of the membrane, and the associated protein functions (10,11). A large experimental effort has been devoted to mapping lipid biosynthetic pathways by characterizing and mutating particular enzymes. There is also an increasing body of experiments that measure the relationship between the biophysical properties of lipids and enzyme activity (10,12). However, there have been few attempts (13) to consider theoretically the interdependence of these two phenomena by modeling the lipid biosynthetic network as an integrated system in which the biochemical and the biophysical descriptions of the metabolic network are fundamentally linked. The focus of the model presented here is to provide a set of tools to understand the interplay between the enzymes and lipids involved in lipid metabolism in relation to the biophysical properties of the bilayer.

Fig. 1 depicts a simplified representation of the connection between the chemical structure of lipids and the mechanical properties of a lipid monolayer. A lipid monolayer consists of conformationally flexible lipids, whose amphiphilic nature leads to a nonuniform pressure distribution across the monolayer. The lateral pressure profile  $\pi(z)$  determines the average “molecular shape” that a lipid adopts and, more importantly,  $J_s$ , the monolayer spontaneous curvature.  $J_s$  is an intrinsic property of a lipid species that corresponds to the monolayer curvature in which a lipid in the monolayer is at the conformation with minimum free energy (14). The spontaneous curvature reflects the desire of a lipid monolayer to either curve away from, or curve toward, the membrane-water interface and whether a lipid is a bilayer or nonbilayer lipid.

A lipid bilayer is formed by two monolayers back-to-back. This arrangement means that the monolayers may not be able

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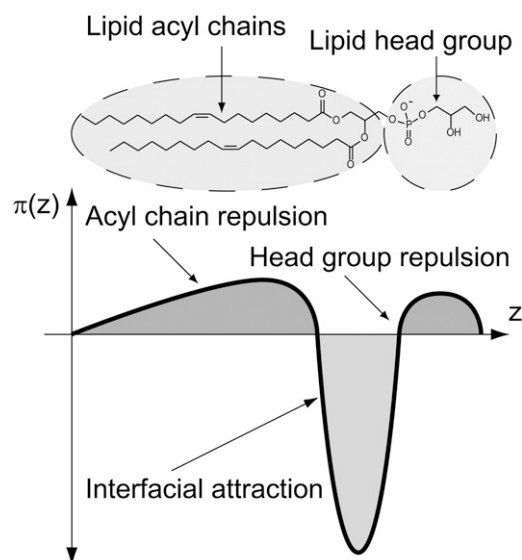


FIGURE 1 Forces that act between lipids at different depths include electrostatic and hydrogen bond interactions at the headgroup, interfacial tension at the hydrophilic-hydrophobic interface, and the packing of the hydrocarbon chains. The lateral pressure profile  $\pi(z)$  depends crucially on the chemical nature of the lipid head group and the length and saturation of the lipid hydrocarbon chains. The lateral pressure profile determines the spontaneous curvature  $J_s$  of a lipid monolayer (14).

to adopt their preferred curvature,  $J_s$ , since the monolayers in the bilayer are held together by the hydrophobic effect. This leads to a difference between the actual curvature of a monolayer, as given by the principal curvatures  $c_1$  and  $c_2$ , and its spontaneous curvature,  $J_s$  (15). Based on this physical picture, Helfrich (16) formulated the stored elastic energy per unit area,  $g$ , of a lipid monolayer that is constrained to have principal curvatures  $c_1$  and  $c_2$ :

$$g = \frac{F}{A} = \frac{\kappa_M}{2}(c_1 + c_2 - J_s)^2,$$

where  $F$  is the Helmholtz free energy,  $A$  is the area, and  $\kappa_M$  is the bending rigidity of the monolayer. The lipids are at the free energy minimum, when the total curvature,  $c_1 + c_2$ , is at the value of the spontaneous curvature  $J_s$ . Because at equilibrium  $g$  is minimized, this means it is more difficult for lipids with large spontaneous curvatures to form a bilayer, which is a flat conformation with small  $c_1$  and  $c_2$ . Indeed, it has been suggested that lipids with  $J_s < -1/6 \text{ nm}^{-1}$  (the negative sign is a convention to denote that the monolayer curves toward water in an interface) do not form bilayers. Instead, they form curved mesophases, such as the inverse hexagonal phase, which are porous (17).

From a biological perspective, porous mesophases would have severe consequences for cellular function and survival. Gruner (3) hypothesized that the average spontaneous curvature  $J_s^{\text{mix}}$  of the lipids in the plasma membrane must be tightly regulated to ensure that the membrane lipids form a (nonporous) bilayer and that the cell is able to control  $J_s^{\text{mix}}$

(15) by modifying its lipid composition through the biochemical networks of lipid metabolism.

This insight has been confirmed experimentally. Lipid extracts from the cell-wall-less Mycoplasma *Acholeplasma laidlawii* grown under different conditions have average spontaneous curvatures  $J_s^{\text{mix}}$  in the small range between  $-1/6.6 \text{ nm}^{-1}$  and  $-1/8.1 \text{ nm}^{-1}$  even though the membrane contains lipids with  $J_s$  outside of this range (18). To achieve this robust regulation, *A. laidlawii* alters the ratio of its two main glucolipids in response to the length and saturation of exogenously fed fatty acids (5), thus maintaining  $J_s^{\text{mix}}$  in a biologically viable “bilayer range” that ensures membrane integrity yet with enough stored elastic energy to allow for its dynamical behavior. Remarkably, although the average spontaneous curvature is controlled, the lipid concentrations exhibit wide variations. This suggests that the control of  $J_s^{\text{mix}}$  is not achieved by targeting specific lipid compositions. These observations also apply to *Escherichia coli* lipid extracts, which begin to form nonbilayer structures close to physiological conditions (7).

Biophysical control mechanisms integrated into lipid biosynthetic networks have been the subject of intense experimental study. An example is given by cytidine triphosphate/phosphocholine cytidyltransferase (CCT), an enzyme involved in the biosynthesis of the ubiquitous lipid phosphatidylcholine. CCT is inactive in the cytoplasm, but becomes active when membrane-bound. It has been shown that its activity is affected by the stored elastic energy in the membrane (12). The biophysical control mechanism arises from the presence of an amphipathic  $\alpha$ -helix that affects enzyme activity by regulating the binding of CCT to lipid bilayers. In a broad sense, the amphipathic  $\alpha$ -helix can be viewed as a “sensor” of the spontaneous curvature since it binds preferentially to lipid bilayers with large negative  $J_s^{\text{mix}}$ , thus modulating the activity of the lipid biosynthetic enzyme. This biophysical control mechanism is chemically nonspecific, as it is based on a biophysical interaction between the enzyme and the membrane, and appears to be generic to a number of enzymes present in lipid biosynthetic pathways (12,19), including those present in *A. laidlawii*, which is the focus of this study.

We have developed a modeling framework for the lipid biosynthetic pathways in *A. laidlawii*. Building upon the *A. laidlawii* biochemical network studied in detail by the groups of Lindblom, Rilfors, and Wieslander (5,6,19,20), we formulate a biophysical mechanism, based upon some of the conceptual foundations established in CCT (12), that couples the activity of lipid biosynthetic enzymes to the membrane composition. Our results show that the presence of feedback increases the robustness of the steady state of the system to parameter variations, in the sense that it decreases the probability of inviable values of  $J_s^{\text{mix}}$  that would lead to porous phases. From a sensitivity analysis, we identify the enzymes that are most efficient in implementing the control of the network. We also study the restrictions that the network imposes on the steady-state concentrations of particular lipids

and show that the system keeps a balance between bilayer and nonbilayer lipids. Finally, we consider the influence of the length of the amphipathic  $\alpha$ -helix on the efficacy of the feedback.

## THE LIPID BIOSYNTHETIC NETWORK OF *A. LAIDLAWII*

We take the cell-wall-less *Mycoplasma A. laidlawii* as our system for the study of cellular models of lipid biosynthesis. This simple organism, which has been studied in great detail (5,6), has two features that make it ideal to showcase our modeling framework. First, virtually all the lipids in *A. laidlawii* are in the plasma membrane (21). This simplifies the model to a single lipid bilayer, avoiding the complexity of cell walls and intracellular compartments. Second, *A. laidlawii* cannot synthesize unsaturated fatty acids and is very limited in its synthesis of saturated fatty acids (5). Therefore, *A. laidlawii* exhibits a significantly reduced number of chemical species in the plasma membrane as it relies on exogenously fed fatty acids for lipid biosynthesis.

The limited fatty acid synthesis implies that the only response of *A. laidlawii* to variations in its fatty acid diet is to alter the composition of the headgroups of the lipids in the membrane through the network of enzymatic reactions represented in Fig. 2. Indeed, experiments show that the membrane lipid composition of *A. laidlawii* depends strongly on the length and saturation of exogenously fed fatty acids (5). When *A. laidlawii* is fed palmitic acid (a short, saturated fatty acid), monoglucosyldiacylglycerol (MGlcDAG) is the most abundant lipid; whereas when *A. laidlawii* is fed oleic acid (a long, unsaturated fatty acid), diglucosyldiacylglycerol (DGlcDAG) dominates. Central to our study is the observation that although the variation in the lipid composition can be large, the cell maintains the average monolayer spontaneous curvature of the plasma membrane  $J_s^{\text{mix}}$  within a “window” in which the bilayer phase is stable (7) (Table 1). The lipid biosynthetic network is able to adjust the lipid composition to achieve a  $J_s^{\text{mix}} > -1/6 \text{ nm}^{-1}$ , thus maintaining a dynamic, yet impermeable plasma membrane.

### The lipid biosynthetic network: biochemical and biophysical descriptions

The biochemical description of the lipid biosynthetic network of *A. laidlawii* is presented in Fig. 2 A. The first step in the metabolic network is, as in other organisms, the acylation of soluble glycerol-3-phosphate (G3P) to form phosphatidic acid (PA) (22). The network then branches out into two pathways.

The upper branch is the phosphatidylglycerol (PG) pathway, well-studied in bacteria, in which PA is converted into PG through the intermediates cytidine diphosphate diacylglycerol (CDP-DAG) and phosphatidylglycerolphosphate (PGP). The corresponding enzymes CDP-DAG synthase (CDS),

PGP synthase (PGPS), and PGP phosphatase (PGPP) have been characterized in *E. coli* (23,24) and in *Clostridium perfringens* (25,26).

The lower branch is a specific pathway in *A. laidlawii*, deduced from the discovery and purification of the PA phosphatase (PAP) (27) and the two consecutive glucosyltransferases, MGlcDAG synthase (MGS) (28) and DGlcDAG synthase (DGS) (29). The final enzymatic reaction is yet to be characterized since the glycerophosphoryl-DGlcDAG (GPDGlcDAG) synthase (GPDGS) that catalyzes the production of GPDGlcDAG has not been purified yet. However, the genetic similarity of MGS and DGS to the enzymes of Gram-positive bacteria (30) suggests that GPDGlcDAG could be synthesized by the transfer of G3P from PG to DGlcDAG, a reaction that occurs in the synthesis of lipoteichoic acids in the cell walls of Gram-positive bacteria (31).

Fig. 2 B presents a biophysical interpretation of the network, showing how the molecular shape of each lipid is reflected in its monolayer spontaneous curvature. This physical picture shows that the position of nonbilayer lipids ( $J_s < -1/6 \text{ nm}^{-1}$ ) and bilayer lipids ( $J_s > -1/6 \text{ nm}^{-1}$ ) within the network has an effect on which enzymes can exercise effective control of the  $J_s^{\text{mix}}$  of the plasma membrane. By inspection, MGS and DGS are good candidates for the control of  $J_s^{\text{mix}}$ , since MGS and DGS catalyze the reactions that lead from the lipid with the most negative  $J_s$  (DAG) to the lipid with the least negative  $J_s$  (DGlcDAG) (Fig. 2 B). This intuition is reinforced by a structural feature of these enzymes. MGS and DGS are both peripheral membrane proteins that translocate between the cytoplasm and the membrane. It is postulated that they are only active when they are inserted into the membrane, as suggested by the increased activity of both MGS (29) and DGS (32) in the presence of lipids with large negative  $J_s$ . This picture leads to a biophysical, intrinsic mechanism for MGS and DGS to control lipid biosynthesis as a function of the average monolayer spontaneous curvature of the membrane. Our model is a mathematical formulation of these ideas.

### Cellular model of lipid biosynthesis

The biochemical constituents of our cellular model of lipid biosynthesis are the membrane lipids, the lipid biosynthetic enzymes, and the soluble cytoplasmic reactants. The membrane lipids are assumed to be homogeneously distributed over both monolayers of the plasma membrane. Although labeling studies in *E. coli* show that lipid biosynthesis occurs mainly at the inner leaflet of the plasma membrane (33), we will assume that lipid transport from the inner to the outer leaflet of the membrane maintains a symmetric bilayer. Our assumption of spatial homogeneity for the lipids is based on the fast lateral diffusion of lipids in bilayers (34,35) and leads to a description in terms of ordinary differential equations. The soluble reactants (such as the nucleotide CTP or the inorganic phosphate ions  $P_i$  and  $PP_i$ ) are assumed to have

**TABLE 1** Spontaneous curvature and lipid composition of *A. laidlawii* grown in oleic acid

Lipid	PA	CDP-DAG	PGP	PG	DAG	MGlcDAG	DGlcDAG	GPDGlcDAG
$J_s$ (nm <sup>-1</sup> )	-1/4.3	0	0	-1/8.7	-1/1.01	-1/2.5	-1/13.1	-1/7.7
Reference	(67)	*	*	(66)	(39)	(18)	(18)	*
$L_{exp}$ (mol %)	0.7 <sup>†</sup>	0.04 <sup>†</sup>	0.04 <sup>†</sup>	15.1	0.7 <sup>†</sup>	7.8	54.4	21.2

\*These  $J_s$  values are estimated. See Appendix A for a discussion.

<sup>†</sup>These lipid molar fractions were below the detection limit and are estimated. See Appendix A.

constant, regulated cytoplasmic concentrations, due to their involvement in general cellular processes. Therefore, they are only parameters (not variables) of the model.

The *A. laidlawii* lipid biosynthetic network is modeled as a system of nonlinear differential equations for eight lipids with seven enzymatic reactions. The variables of the model are compiled into the vector of lipid surface concentrations expressed in molar fraction:  $\mathbf{L}^T = [\{PA\} \{CDP-PAG\} \{PGP\} \{PG\} \{DAG\} \{MGlcDAG\} \{DGlcDAG\} \{GPDGlcDAG\}]$ . The sum of the lipid molar fractions is 1 at all times:  $\mathbf{1}^T \mathbf{L} = 1$ .

Each enzymatic reaction has a nonlinear rate equation of the Michaelis-Menten type, modified using surface dilution kinetics, as explained below, to account for the fact that the reactions take place on the membrane. The enzyme rate equations are compiled into a vector  $\mathbf{v}^T = [v_{CDS} v_{PGPS} v_{PGPP} v_{PAP} v_{MGS} v_{DGS} v_{GPDGS}]$ . The modulation of the enzyme activity due to the biophysical interaction with the mechanical properties of the membrane is introduced through a diagonal matrix  $K_a = \text{diag}([K_{a,CDS} K_{a,PGPS} K_{a,PGPP} K_{a,PAP} K_{a,MGS} K_{a,DGS} K_{a,GPDGS}])$ , which incorporates the possibility that some of the enzymatic rates, specifically those of MGS and DGS, could depend on  $J_s^{\text{mix}}$ . If the enzyme is curvature sensitive, its association constant  $K_{a,Enzyme}$  will depend on  $J_s^{\text{mix}}$ . Otherwise, the corresponding  $K_{a,Enzyme} = 1$ . This is the basis of the biophysical feedback mechanism, which will be introduced in the following section.

The topology of the reaction network is encoded in a stoichiometric matrix  $N$ , where  $N_{ij}$  is the number of lipid species  $i$  consumed (negative) or produced (positive) in reaction  $j$ :

$$N = \begin{pmatrix} -1 & 0 & 0 & -1 & 0 & 0 & 0 \\ 1 & -1 & 0 & 0 & 0 & 0 & 0 \\ 0 & 1 & -1 & 0 & 0 & 0 & 0 \\ 0 & 0 & 1 & 0 & 0 & 0 & -1 \\ 0 & 0 & 0 & 1 & -1 & 0 & 1 \\ 0 & 0 & 0 & 0 & 1 & -1 & 0 \\ 0 & 0 & 0 & 0 & 0 & 1 & -1 \\ 0 & 0 & 0 & 0 & 0 & 0 & 1 \end{pmatrix}.$$

The matrix  $N$  accounts for the enzymatic reactions and ensures mass conservation. However, our cellular model must also include both the lipid degradation into soluble products and the lipid insertion that enables a growing cell to double the number of lipids before cell division. These processes are incorporated through the transport vector  $\mathbf{t}$  and

the normalization vector  $\mathbf{n}$ . The transport vector  $\mathbf{t}$  encapsulates the balance of lipids inserted and extracted. In our model, only PA is inserted at a constant cellular rate  $V_{+,PA}$  and lipid degradation is assumed not to play a significant role in *A. laidlawii* lipid metabolism (36). Therefore,  $\mathbf{t}^T = [V_{+,PA} \ 0 \ 0 \ 0 \ 0 \ 0 \ 0 \ 0]$ .

The normalization vector  $\mathbf{n}$ , given by

$$\mathbf{n} = -(\mathbf{1}^T \mathbf{t}) \mathbf{L},$$

reduces the surface concentration of each lipid in proportion to its molar fraction while at the same time maintaining the sum of the molar fractions equal to 1.

Combining all the terms, the model can be written compactly as

$$\frac{d\mathbf{L}}{dt} = NK_a(J_s^{\text{mix}}) \mathbf{v}(\mathbf{L}) + \mathbf{t} + \mathbf{n}. \quad (1)$$

This system has stationary points  $\mathbf{L}^*$ .

Finally, to close the system, we need to relate  $J_s^{\text{mix}}$  to the lipid concentration. Our underlying, linear assumption is that  $J_s^{\text{mix}}$  is well approximated by the weighted average of the spontaneous curvatures of the individual lipids:

$$J_s^{\text{mix}} = \mathbf{J}_s^T \mathbf{L}. \quad (2)$$

This linear assumption has been shown experimentally to lead to an accurate approximation of the phase behavior of lipid mixtures (37). This linear assumption is also used in many of the experiments that measure the  $J_s$  of neutral and anionic lipids (38–41). Using Eq. 2 with the  $J_s$  values and experimental lipid composition  $\mathbf{L}_{exp}$  in Table 1 leads to a calculated  $J_s^{\text{mix}}$  of  $-1/7.9 \text{ nm}^{-1}$ , which lies within the measured range from  $-1/6.6 \text{ nm}^{-1}$  to  $-1/8.1 \text{ nm}^{-1}$  of *A. laidlawii* lipid extracts.

### Functional form of the lipid biosynthetic enzyme kinetic rates, $\mathbf{v}(\mathbf{L})$

Before considering the biophysical mechanism that couples the biochemical reactions to the mechanical properties of the membrane, we state first some specific features of the enzyme kinetic rate equations of the membrane lipid network. The functional form of the rate equations  $\mathbf{v}(\mathbf{L})$  in the model differs from standard enzyme kinetics (42) in two respects. First, our cellular model must take into account the number of copies of the enzyme in the cell. Second, we must account for the fact



that lipid biosynthetic enzymes have soluble, cytoplasmic reactants that diffuse in three dimensions, whereas their lipid reactants diffuse within the two-dimensional membrane.

Kinetic studies (27–29) have fitted the rates of *A. laidlawii* lipid biosynthetic enzymes to surface-dilution kinetics, in which soluble reactants have a bulk concentration in units of molarity and membrane reactants have a surface concentration in (dimensionless) molar fraction (43). All of the enzymatic reactions in the network, except for the reaction catalyzed by CDS, can be assumed to be irreversible. There is experimental evidence that supports this assumption, e.g., the hydrolyses of the phosphoanhydride bonds in PA and PGP are irreversible (44). Therefore, the rate equations for  $v_{\text{PGPS}}$ ,  $v_{\text{PGPP}}$ ,  $v_{\text{PAP}}$ ,  $v_{\text{MGS}}$ , and  $v_{\text{DGS}}$  are of the form

$$v_{\text{Enzyme}} = V_{\text{cell}} \frac{\frac{\{L\}_i [S]}{K_{\text{mL}} K_{\text{mS}}}}{1 + \frac{\{L\}_i}{K_{\text{mL}}} + \frac{[S]}{K_{\text{mS}}}}, \quad (3)$$

where  $\{L\}_i$  is the surface concentration of the lipid substrate (in molar fraction) and  $[S]$  is the bulk concentration of the soluble substrate (in units of molarity). Similarly,  $K_{\text{mL}}$  is the Michaelis constant of  $\{L\}_i$  (in molar fraction) and  $K_{\text{mS}}$  is the Michaelis constant of  $[S]$  (in units of molarity). Experimental values of the enzyme kinetic constants are listed in Appendix B.

Note that  $V_{\text{cell}}$  is the rate for all copies of the enzyme in the cell (in units of molar fraction/min):

$$V_{\text{cell}} = \frac{M_{\text{Enzyme}}}{N_{\text{Lipid}}} V_{\text{max}}, \quad (4)$$

where  $M_{\text{Enzyme}}$  is the total mass of each enzyme in the cell and  $N_{\text{Lipid}}$  is the number of moles of lipid in the cell.  $V_{\text{max}}$  is the standard Michaelis-Menten limiting rate, which typically has units of moles of product synthesized per milligrams of enzyme per minute (42). It is assumed that the ratio  $M_{\text{Enzyme}}/N_{\text{Lipid}}$  is kept constant in a growing cell over the cell cycle. In Appendix B we show how we have estimated these parameters.

Two of the enzymatic reactions have slightly different functional forms. The final reaction of the lower path, catalyzed by GPDGS, although irreversible, involves two lipid substrates. As mentioned above, the CDS reaction is modeled reversibly since the equilibrium constant is much less than 1 (23). The rate equations of these reactions are listed in Appendix B.

### Spontaneous-curvature-sensitive enzymes

We now introduce the terms in the model that describe how the activity of an enzyme with an amphipathic  $\alpha$ -helix is modulated as a function of spontaneous curvature, which is in turn a function of the lipid composition. As mentioned above, there is extensive evidence that supports the theory that the activity and function of many proteins, both integral and

peripheral, are regulated by the biophysical properties of biological membranes (10,35). Such phenomena differ markedly from specific protein-lipid interactions. Although our model deals with the binding of an amphipathic  $\alpha$ -helix to the membrane, the mechanism could be extended to describe the binding of other amphipathic motifs to the membrane.

Enzyme kinetic studies have shown that lipids with large negative  $J_s$  increase the activity of both MGS (29) and DGS (32). MGS has an amphipathic  $\alpha$ -helix between residues 67 and 85 (30,45), that shares 5 of its first 8 residues with an  $\alpha$ -helix of the *E. coli* division-site-selection protein MinD (46) that targets heterologous proteins to the membrane (47). Since it has been shown that MGS (19,29), the MGS amphipathic  $\alpha$ -helix (20), and the MinD amphipathic  $\alpha$ -helix (48) all preferentially bind to membranes with large negative  $J_s^{\text{mix}}$ , we hypothesize that the curvature-sensitive activity of MGS is a result of the membrane binding of this  $\alpha$ -helix.

Through surface plasmon resonance (SPR) experiments, it has been concluded that liposomes bind to MGS through a two-step process (19). The first binding step is independent of lipid composition and has a dissociation constant of  $\sim 10$  nM. The second binding step has a large dependence on lipid composition, as its dissociation constant decreases from 10 mM to 100 nM when the liposomes have large negative  $J_s^{\text{mix}}$  (19). Since liposomes with large  $J_s^{\text{mix}}$  increase both the activity of MGS and the strength of the second binding step, it follows that MGS is only active after the second binding step.

Amphipathic peptides form random coils in solution. The first binding step corresponds to surface adhesion induced by the electrostatic attraction of exposed basic residues to acidic membrane lipids. The second, subsequent step is the insertion of the hydrophobic residues into the membrane coupled with the emergence of the  $\alpha$ -helix, which is entropically favored by the hydrophobic membrane environment. This two-step membrane binding (49) can be summarized through a simple kinetic mechanism,



where  $K_{d1}$  and  $K_{d2}$  are the dissociation constants of the binding steps. At steady state, the fraction of membrane-inserted amphipathic  $\alpha$ -helices that result in active enzymes is given by the association constant

$$K_a = \frac{1}{1 + K_{d2} + K_{d1}K_{d2}}. \quad (5)$$

We now derive expressions for  $K_{d1}$  and  $K_{d2}$  from biophysical considerations.

#### First binding step, $K_{d1}$

From SPR studies,  $K_{d1}$  is measured to be  $\sim 10$  nM (19). It is proposed that this first (irreversible) binding is a result of electrostatic attraction. Structurally, the presence of eight

positively charged residues on the 19-residue amphipathic  $\alpha$ -helix (see Fig. 4 B) will produce a strong electrostatic attraction. Indeed, there is ample evidence that negatively charged anionic lipids are essential for the binding and activity of MGS. For instance, it is known that shielding the anionic lipids with 0.75 M NaCl prevents the binding of MGS (19).

From simple electrostatic considerations,  $K_{d1}$  is given by the Boltzmann relation,

$$K_{d1} = \exp\left(\frac{z_p e \psi_0}{k_B T}\right), \quad (6)$$

where  $z_p e = +8e$  is the net charge of the amphipathic  $\alpha$ -helix and  $\psi_0$  is the membrane surface potential. A dissociation constant of 10 nM would imply  $\psi_0 \cong -60$  mV at 40°C, which is comparable to the measured membrane surface potentials of bacterial lipid bilayers (50). This simple estimate reinforces the plausibility of the interpretation of the first binding step in terms of electrostatic interactions. Clearly, the biophysical picture will be complex, including the shielding of charges on the peptide to give an effective valence (51) and the likely involvement of other positively charged enzyme domains.

#### Second binding step, $K_{d2}$

The second binding step involves at least three energetic processes: membrane insertion of the hydrophobic residues; peptide folding to form the  $\alpha$ -helix; and lipids bending to accommodate the inserted  $\alpha$ -helix. It has been observed that  $K_{d2}$  decreases dramatically along the lipid sequence dioleoylphosphatidylglycerol (DOPG) > cardiolipin (CL) > dioleoylphosphatidylethanolamine (DOPE) > dioleoylglycerol (DOG) (19), i.e., as  $J_s$  becomes more negative (39,52). This is

the basis for our assumption that the second binding step is dominated by the energy of lipids bending to accommodate the helix.

We can understand this process through the following simplified biophysical picture. Consider a locally flat bilayer with average monolayer spontaneous curvature  $J_s^{\text{mix}}$ . The diameter of the  $\alpha$ -helix is comparable to that of a lipid. Consequently, the insertion of an amphipathic  $\alpha$ -helix into a flat membrane does not result in a change of the monolayer curvature, yet it leads to a change in the molecular shape of the lipids alongside the  $\alpha$ -helix (12) (Fig. 3 A). This would translate into a monolayer curvature,  $c_{\text{bound}} \neq 0$ , for a monolayer formed entirely by lipids like those surrounding the amphipathic  $\alpha$ -helix.

Fig. 3 A sketches a very simple geometrical argument to obtain a first-order estimate of  $c_{\text{bound}}$ :

$$c_{\text{bound}} = -1/R_{\text{bound}} = \frac{-r}{\sqrt{A(r^2 + t^2)}}, \quad (7)$$

where  $r = 0.45$  nm is the radius of the  $\alpha$ -helix (53);  $t$  is the monolayer thickness (the distance between the middle of the  $\alpha$ -helix and the bilayer midpoint), which is measured to be 1.71 nm (53); and  $A$  is the average interfacial surface area of the *A. laidlawii* lipids, which is measured to be 0.65 nm<sup>2</sup> (5).  $A$  is assumed to be square and the pivotal plane is assumed to coincide with the middle of the  $\alpha$ -helix. Equation 7 gives an estimated  $c_{\text{bound}} \approx -1/3.2$  nm<sup>-1</sup>, which is significantly nonflat.

The cylindrical deformation of the  $\alpha$ -helix ensures that one of the principal curvatures is zero,  $c_2 = 0$ . Therefore, the change in the stored elastic energy in Eq. 1 due to the bending of the lipids alongside the amphipathic  $\alpha$ -helix is

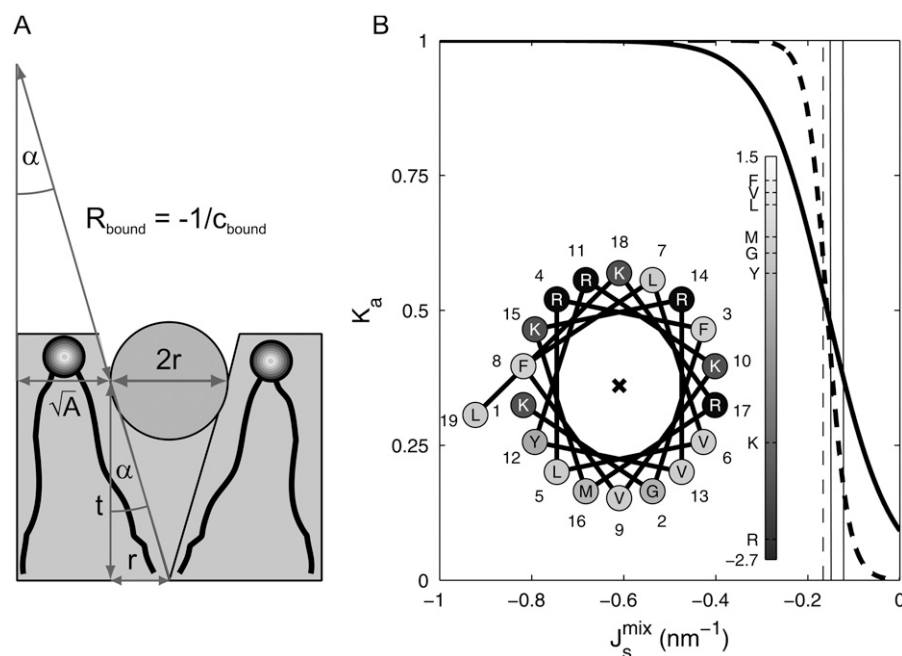


FIGURE 3 (A) Geometric argument used to calculate  $c_{\text{bound}}$ , the curvature of a lipid monolayer consisting entirely of lipids that lie alongside an amphipathic  $\alpha$ -helix. (B) Association constant  $K_a$  as a function of  $J_s^{\text{mix}}$  for a 19-residue  $\alpha$ -helix (dark solid line) and, for a 58-residue  $\alpha$ -helix, such as that of CCT, plotted for comparison (dark dashed line). The dashed vertical line is  $J_s = -1/6$  nm<sup>-1</sup> and the solid vertical lines give the measured range of  $J_s^{\text{mix}}$  of lipid extracts (5). (Inset) Helical-wheel projection of residues 67–85 of MGS. The bar gives the Eisenberg consensus normalized hydrophobicity scale (76).

$$F(c_1 = c_{\text{bound}}) - F(c_1 = 0) = N_h A \frac{\kappa_M}{2} c_{\text{bound}} (c_{\text{bound}} - 2J_s^{\text{mix}}), \quad (8)$$

where  $\kappa_M$  is the bending rigidity of lipids, which we take to be  $10 k_B T$  (38), and  $N_h = 7.1$  is the number of lipids that adopt curvature  $c_{\text{bound}}$  along both sides of the amphipathic  $\alpha$ -helix.  $N_h$  is calculated for a 19-residue  $\alpha$ -helix of length 2.85 nm with 3.5 lipids of length  $0.65^{1/2}$  nm along each side of its long axis. For the range of  $J_s$  values in Table 1, the free energy is between  $-1.7 k_B T/\text{lipid}$  and  $0.2 k_B T/\text{lipid}$ . These energies are not large enough to cause the lateral sequestration of lipids around the  $\alpha$ -helix (54), thus justifying the use of  $J_s^{\text{mix}}$ .

Equation 9 provides an estimate for the binding energy if we assume that the main energetic contribution to this process comes from lipid bending. The dissociation constant of the second binding step would then be given by the Boltzmann relation:

$$K_{d2} = \exp\left(N_h A \frac{\kappa_M}{2} c_{\text{bound}} (c_{\text{bound}} - 2J_s^{\text{mix}}) / k_B T\right). \quad (9)$$

Note that for the range of  $J_s$  values in Table 1, the modeled  $K_{D2}$  ranges between 4 M and 5  $\mu\text{M}$ . The difference with the experimental values of  $K_{D2}$  may be explained by the enhanced electrostatic attraction due to the absence of divalent cations and the use of zwitterionic lipids in the SPR experiments (19,20). Note that when  $J_s^{\text{mix}} = c_{\text{bound}}/2 = -1/6.3 \text{ nm}^{-1}$ , the binding energy is zero and MGS is equally likely to be bound or unbound. Reassuringly, this bound-to-unbound transition is centered at a value of  $J_s^{\text{mix}}$  that lies between the formation of nonbilayer structures and the lower bound of the experimental curvature of lipid extracts in *A. laidlawii*:  $-1/6 < c_{\text{bound}}/2 < -1/6.6$  (Table 1).

Equations 6 and 9 provide the biophysical feedback for the system in Eq. 1, as the association constant  $K_{a,\text{MGS}}$  multiplies the rate  $v_{\text{MGS}}$ . Given the individual lipid spontaneous curvatures  $J_s$  in the system (Table 1), and assuming a constant  $K_{d1} = 10 \text{ nM}$ , the association constant is constrained to be in the range  $1 \geq K_{a,\text{MGS}} \geq 0.23$  (Fig. 3 B), and the 19-residue  $\alpha$ -helix provides a fourfold regulation of MGS activity. At large negative  $J_s^{\text{mix}}$ , almost all MGS is active and the synthesis of MGlcDAG increases  $J_s^{\text{mix}}$ . The opposite effect is produced when  $J_s^{\text{mix}}$  is less negative. Clearly, a longer amphipathic  $\alpha$ -helix would produce significantly stronger regulation of activity (Fig. 3 B).

### Parameter estimation for the model

The time evolution of the system in Eq. 1 and its corresponding stationary point depend on the model parameters. Most of these parameters have been collected from an extensive survey of the literature, or have been estimated or measured directly. As is usual in the literature, some of the parameters carry substantial uncertainty. In addition, there is an absence of kinetic parameters for some of the enzymes of the *A. laidlawii* lipid biosynthetic network.

To complete our parametric description, we carry out a constrained nonlinear parameter estimation in which we search for the positive parameter set  $\mathbf{p}$  that reproduces the experimentally observed lipid concentrations  $\mathbf{L}_{\text{exp}}$  as close as possible while minimizing the distance to the reliable literature values. Our method of choice to solve this constrained optimization is the Stochastic Ranking Evolutionary Strategy (SRES) (55), an evolutionary strategy with stochastic ranking, which has been shown in a recent survey (56) to be successful in finding feasible parameters in nonlinear biochemical pathways.

For such an underdetermined system, a multiobjective optimization is pursued. The primary objective is to minimize the difference between  $\mathbf{L}^*(\mathbf{p})$ , the stationary point of the model in Eq. 1 for the parameter set  $\mathbf{p}$ , and the experimentally observed lipid composition  $\mathbf{L}_{\text{exp}}$  given in Table 1,

$$\|\mathbf{L}^*(\mathbf{p}) - \mathbf{L}_{\text{exp}}\|^2.$$

The secondary objective is to minimize the difference between the estimated parameter set  $\mathbf{p}$  and the literature parameters  $\mathbf{p}_{\text{lit}}$ . Instead of minimizing the Euclidean norm  $\|\mathbf{p} - \mathbf{p}_{\text{lit}}\|$ , in our case we minimize a more appropriate measure of the relative distance between the parameter sets, previously introduced to quantify the robustness of dynamical systems (57),

$$\sum_j c_j \left| \log_{10} \left( \frac{p_j}{p_{\text{lit},j}} \right) \right|,$$

i.e., the sum of the absolute logarithmic errors between  $\mathbf{p}$  and  $\mathbf{p}_{\text{lit}}$  weighted by  $c_j$ , the confidence in the  $j$ th literature parameter. In particular, parameters obtained from *A. laidlawii* experiments have been assigned  $c_j = 1$ , whereas  $c_j = 1/2$  for parameters taken from experiments on other organisms, such as *E. coli*. As a check that the combination of our model and this multiobjective estimation procedure produces plausible parameter sets, we have verified that we can obtain parameters for which the model reproduces all the different lipid compositions that have been observed experimentally (5).

There are a total of 25 kinetic parameters in the model, of which only 18 have literature values. We run our multiobjective optimization by varying 15 parameters (the 7 unknown and 8 parameters with uncertain literature values) and obtain the estimated parameter set  $\mathbf{p}_0$  presented in Table 2. The distance between each estimated parameter and its literature value has been constrained to be at most two orders of magnitude. The estimated parameter set reflects the sensitivity of the steady state to particular parameters, specifically those appearing in the numerator of the rate equations:  $V_{\text{cell,Enzyme}}$  and the soluble substrate concentrations. This emphasizes the importance of measuring intracellular metabolite concentrations.

Our model in Eq. 1 with the estimated parameter set  $\mathbf{p}_0$  in Table 2 will be our reference system henceforth. This system has a stationary point at the experimental lipid composition



**TABLE 2** Model parameters for the reference system

Parameter	Literature ( $p_{lit}$ )	Estimated ( $p_0$ )
$V_{+,PA}, \text{min}^{-1}$	$8.2 \times 10^{-3}$	
$V_{cell,CDS}, \text{min}^{-1} \dagger$	$9.6 \times 10^{-3}$	
$V_{cell,PGPS}, \text{min}^{-1} \dagger$	$4.7 \times 10^{-3}$	
$V_{cell,PGPP}, \text{min}^{-1}$	*	3.2
$V_{cell,PAP}, \text{min}^{-1}$	$4.1 \times 10^{-2}$	$7.7 \times 10^{-2}$
$V_{cell,MGS}, \text{min}^{-1}$	$1.8 \times 10^{-3}$	$1.4 \times 10^{-2}$
$V_{cell,DGS}, \text{min}^{-1}$	$3.5 \times 10^{-4}$	$1.2 \times 10^{-3}$
$V_{cell,GPDGS}, \text{min}^{-1}$	*	$1.5 \times 10^{-2}$
CDS $K_{M,PA}, \text{mol \%}$	*	$9.3 \times 10^{-2}$
PGPS $K_{M,CDPDAG}, \text{mol \%}$	*	$1.0 \times 10^{-2}$
PGPP $K_{M,PGP}, \text{mol \%}$	*	38.2
PAP $K_{M,PGP}, \text{mol \%}$		10
MGS $K_{M,DAG}, \text{mol \%}$	6	5.2
DGS $K_{M,MGlcDAG}, \text{mol \%}$		1
GPDGS $K_{M,PG}, \text{mol \%}$	*	25
GPDGS $K_{M,DGlcDAG}, \text{mol \%}$	*	85
CDS $K_{M,CTP}, \text{mM}^\dagger$		0.58
PGPS $K_{M,G3P}, \text{mM}^\dagger$		0.32
MGS $K_{M,UDP-Glc}, \text{mM}$		0.4
DGS $K_{M,UDP-Glc}, \text{mM}$		0.14
CDS $K_{eqm}$		0.22
CTP, mM		0.5
UDP-Glc, mM $^\dagger$	0.4	2.5
PP <sub>i</sub> , mM $^\dagger$		1
G3P, mM $^\dagger$	0.2	0.32

Parameters are obtained through a multiobjective optimization using the evolutionary algorithm SRES (55). Parameters marked \* have not been measured. Parameters marked  $^\dagger$  correspond to *E. coli* and are given less weight in the optimization. See Appendix B for references and details of the literature parameters.

shown in Table 1, with  $J_s^{\text{mix}} = -1/7.9 \text{ nm}^{-1}$ . In the next section, we explore the effect of the biophysical regulation mechanism introduced above.

## RESULTS

We now investigate the behavior of the cellular model of lipid biosynthesis through the numerical integration of Eq. 1 under a variety of conditions. The first robust feature of the model is that it evolves to a steady state that is independent of the initial condition. Although we have not proved global stability explicitly, numerical integrations from more than  $10^5$  randomly generated initial conditions all converge to the same stationary lipid composition. This is strong evidence that the steady state is globally attracting. Our numerical investigation of the model therefore translates into an evaluation of how the fixed point  $\mathbf{L}^*(\mathbf{p})$  changes in response to variations in the parameters or in the presence of feedback.

### Which enzyme rates most affect $J_s^{\text{mix}}$ ?

Experiments indicating that the activities of both MGS and DGS are curvature-sensitive (28,29) have led to the hypothesis that these two enzymes are responsible for the

control of  $J_s^{\text{mix}}$ . If this is true, the rates of MGS and DGS must have a large effect on the steady-state  $J_s^{\text{mix}}(\mathbf{L}^*)$ . In this section, we use our model to determine which enzymes of the *A. laidlawii* lipid biosynthetic network have the largest effect on  $J_s^{\text{mix}}(\mathbf{L}^*)$  in the absence of feedback. This is an initial step before we introduce the biophysical feedback explicitly in the next section, i.e., in this section the matrix  $K_a$  does not depend on the curvature  $J_s^{\text{mix}}$ .

This question can be posed in the well-known framework of sensitivity analysis, which has been used to characterize, e.g., the robustness of bacterial chemotaxis networks (57). For the reference parameters  $\mathbf{p}_0$  (Table 2), the model evolves to the experimental lipid composition  $\mathbf{L}_{\text{exp}}$  (Table 1), i.e.,  $\mathbf{L}^*(\mathbf{p}_0) = \mathbf{L}_{\text{exp}}$ . However, the parameters  $\mathbf{p}$  are inherently noisy. Specifically, the seven  $V_{\text{cell,Enzyme}}$  have the most influence on the steady state while at the same time having large variability. Therefore, our sensitivity analysis investigates how changes in the different  $V_{\text{cell,Enzyme}}$  translate into variations of the steady-state  $J_s^{\text{mix}}(\mathbf{L}^*)$ .

The sensitivity analysis is performed through Monte Carlo sampling, one enzyme at a time. The  $V_{\text{cell,Enzyme}}$  of the enzyme under study is fixed at the reference value in Table 2. We then produce  $10^6$  parameter sets where the other six  $V_{\text{cell,Enzyme}}$  are drawn from a random distribution conditioned to produce uniform sampling (over the interval [0,6]) of the logarithmic variation of the parameter set,  $k$ :

$$k = \sum_j \left| \log_{10} \left( \frac{p_j}{p_{0j}} \right) \right|. \quad (10)$$

Clearly, this implies that the individual  $V_{\text{cell,Enzyme}}$  parameters are not sampled uniformly (see the *inset* of Fig. 4 A). Effectively, our sensitivity analysis considers variations of up to almost two orders of magnitude in each of the six  $V_{\text{cell,Enzyme}}$ , and an overall uniform variation of six orders of magnitude for the complete parameter set. The fixed point for each of the  $10^6$  parameter sets is obtained and the corresponding  $J_s^{\text{mix}}$  is calculated.

Fig. 4 A shows the results for the enzyme MGS as a two-dimensional histogram of  $P_{\text{MGS}}(J_s^{\text{mix}}, k)$ , the distribution of the  $10^6$  random parameter sets. As expected, the distribution is centered on the reference value of  $J_s^{\text{mix}} = -1/7.9 \text{ nm}^{-1}$  and becomes broader as the variation of the parameter set,  $k$ , grows. Since biophysical experiments show that membranes with  $J_s^{\text{mix}} < -1/6 \text{ nm}^{-1}$  do not form bilayers, we can consider such compositions as biologically nonviable (17). This is marked as a dashed line in Fig. 4 A. Therefore, the distribution  $P(J_s^{\text{mix}}, k)$ , or its marginal  $P(J_s^{\text{mix}})$ , quantifies how likely it is for the system to evolve to a nonbilayer state when a particular enzyme is kept fixed at its reference value and all other enzymes have uncertain  $V_{\text{cell,Enzyme}}$  values. Essentially, this is also a measure of the relevance of the particular enzyme for the controllability of the system, as it quantifies the variability of the output when a given parameter is kept tightly controlled.

The complete results for the system are summarized in Fig. 4 B, where we plot the marginal distributions  $P_{\text{Enzyme}}(J_s^{\text{mix}})$

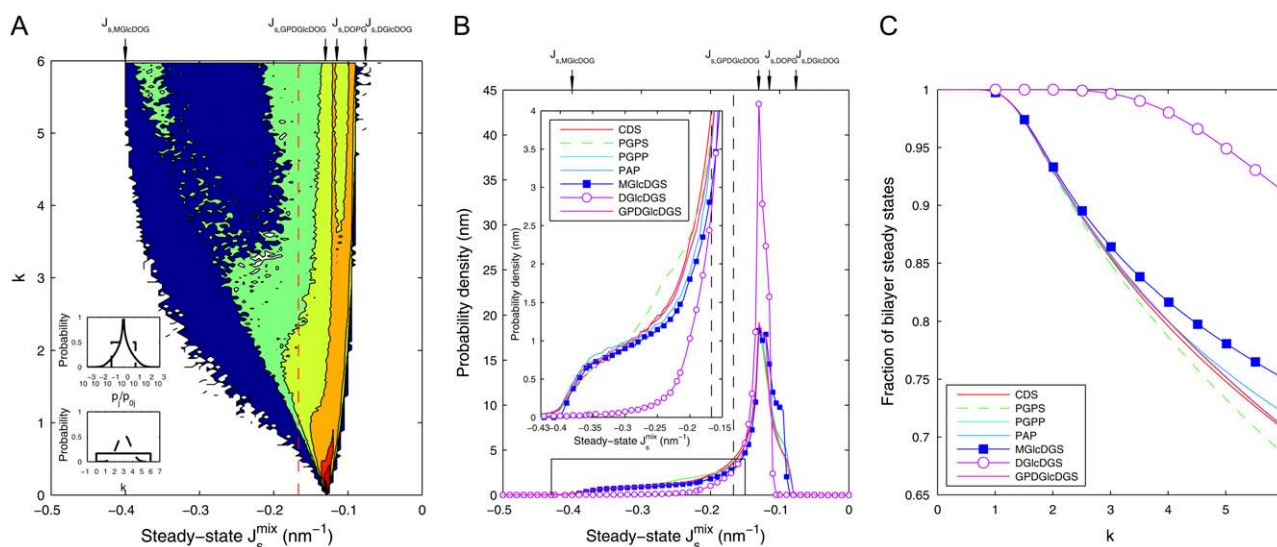


FIGURE 4 (A) Histogram of the distribution  $P_{\text{MGS}}(J_s^{\text{mix}}, k)$  of the steady-state  $J_s^{\text{mix}}$  for a sampling of  $10^6$  random parameter sets, where  $V_{\text{cell,MGS}}$  is fixed and the other six  $V_{\text{cell,Enzyme}}$  values are varied.  $k$  is defined in Eq. 10 and measures the logarithmic variation of the parameter set. The individual  $V_{\text{cell,Enzyme}}$  distribution used (solid, top inset) ensures that the logarithmic variation  $k$  is sampled uniformly (solid, bottom inset). If uniform individual  $V_{\text{cell,Enzyme}}$  distributions were used (dashed, top inset), then  $k$  would approach a Gaussian distribution (dashed, bottom inset). (B) Marginal probability distributions  $P_{\text{Enzyme}}(J_s^{\text{mix}})$  of all seven enzymes, where one  $V_{\text{cell,Enzyme}}$  is fixed, whereas the other six  $V_{\text{cell,Enzyme}}$  are varied. The dashed vertical line indicates the critical value  $J_s^{\text{mix}} = -1/6 \text{ nm}^{-1}$  below which bilayers do not form. (C) Cumulative probability that the steady state will be viable ( $J_s^{\text{mix}} > -1/6 \text{ nm}^{-1}$ ) against the logarithmic variation  $k$  of the state.

for the seven enzymes. All the distributions are centered on the reference  $J_s^{\text{mix}}$  value of  $-1/7.9 \text{ nm}^{-1}$ ; however, the variance and the tails of the distributions differ. Specifically, DGS and MGS (marked with symbols in Fig. 4 B) have much smaller variances and sharper decay tails than the other five enzymes. The left tail of the distribution is relevant as it gives the proportion of biologically inviable stationary states that do not form bilayers. Fig. 4 C shows the fraction of viable steady-state lipid compositions as a function of the variability  $k$ . The results clearly show that keeping the rate of DGS fixed to its reference value is the most efficient way of guaranteeing a viable system.

The reason for this sensitivity is clear if we examine the network in Fig. 2 B. The enzyme DGS catalyzes the synthesis of DGLcDAG, with a small negative  $J_s$ , from MGLcDAG, with a large negative  $J_s$ . Since the membrane binding of amphipathic  $\alpha$ -helices is increased by lipids with large negative  $J_s$ , this provides a direct link with the biophysical feedback mechanism described above. The implication is that enzymes that catalyze reactions that result in a large positive change in  $J_s^{\text{mix}}$  (i.e., DGS and to a lesser extent MGS) are strong candidates to exert the biophysical feedback control of membrane curvature, in accordance with kinetic data. In the next section, the effect of the biophysical feedback provided by the amphipathic motifs is investigated in detail.

### Effect of the biophysical feedback on $J_s^{\text{mix}}$

We now study the effect of the biophysical feedback, mediated by amphipathic  $\alpha$ -helices, on the control of the steady-

state  $J_s^{\text{mix}}$ . Our model encodes this mechanism through the association constants  $K_{\text{a,MGS}}$  and  $K_{\text{a,DGS}}$  collected in the matrix  $K_{\text{a}}(J_s^{\text{mix}})$ .

A sensitivity analysis similar to that performed in the preceding section is carried out to measure how much the variability of the system is reduced in the presence of feedback. We draw  $10^6$  parameter sets from a random distribution of  $V_{\text{cell,Enzyme}}$  such that the logarithmic variation  $k$ , defined in Eq. 10, is uniform over the interval  $[0,7]$ . Fig. 5 A shows four marginal distributions of the steady-state  $J_s^{\text{mix}}$  of the system without feedback and with different combinations of feedback on MGS and DGS. In particular, we model MGS to have a 19-residue amphipathic  $\alpha$ -helix (see Fig. 3 B) and we hypothesize that a similar  $\alpha$ -helix is responsible for the curvature-sensitive activity of DGS, as suggested by secondary-structure predictions (30). The numerics show that the effect of feedback is noticeable in the reduction of the left tail of the distribution. This means that inviable, nonbilayer steady states are less probable when feedback is present. This is especially prominent for DGS, although MGS also contributes to the control of  $J_s^{\text{mix}}$ , as shown in Fig. 5 B. The combined feedback of MGS and DGS reduces the fraction of inviable oleoyl acyl lipid compositions by 19%.

### The robustness of the lipid compositions

A central feature of the biophysical feedback mechanism is the fact that the enzymatic network controls the physical property  $J_s^{\text{mix}}$  and not the steady-state lipid concentrations  $\mathbf{L}^*$ . However,  $J_s^{\text{mix}}$  is a function of the lipid concentrations,

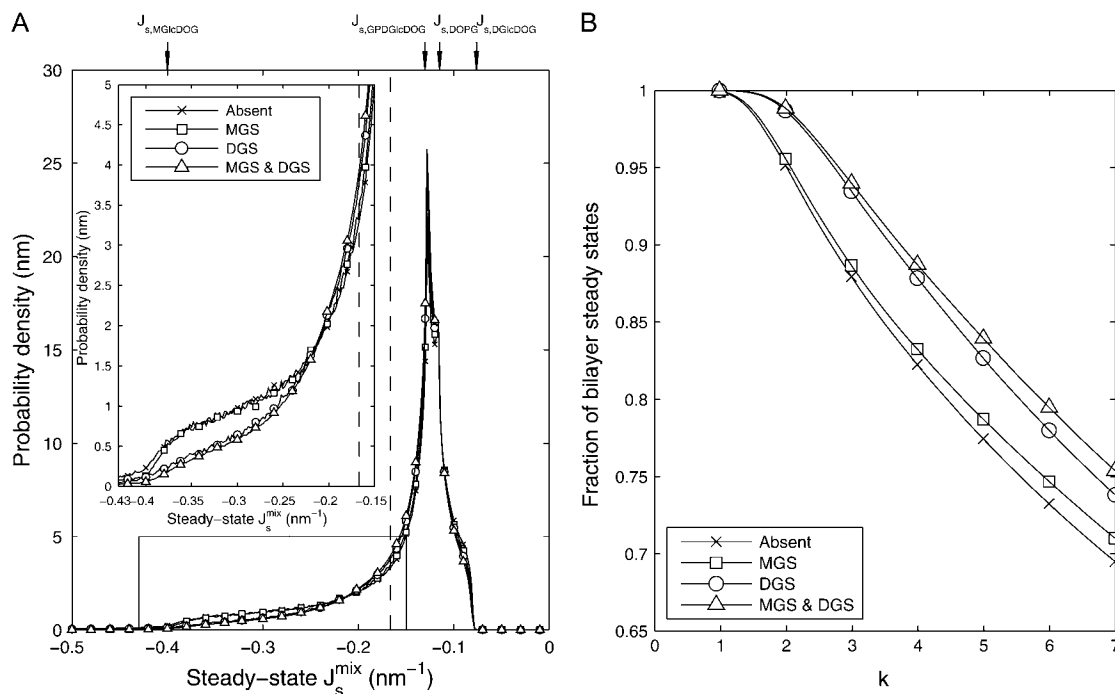


FIGURE 5 (A) Effect of the biophysical feedback on the control of the steady-state  $J_s^{\text{mix}}$ . The four marginal distributions  $P(J_s^{\text{mix}})$ , obtained from  $10^6$  random parameter sets in which all seven enzyme rates  $V_{\text{cell,Enzyme}}$  are varied, show a reduction of the probability of inviable states with  $J_s^{\text{mix}} < -1/6 \text{ nm}^{-1}$ . In the absence of feedback, we fix  $K_{a,\text{MGS}}$  at the reference value of  $K_{a,\text{MGS}}$  ( $J_s^{\text{mix}} = -1/7.9 \text{ nm}^{-1}$ ) shown in Fig. 3 B (×). MGS is modeled to have a 19-residue  $\alpha$ -helix (□), DGS is modeled with a 19-residue  $\alpha$ -helix (○), both MGS and DGS are modeled with 19-residue  $\alpha$ -helices (△). (B) The cumulative probability that the steady state forms a bilayer ( $J_s^{\text{mix}} > -1/6 \text{ nm}^{-1}$ ) as a function of the logarithmic variation  $k$ .

and it is important to study the underlying variability of  $\mathbf{L}^*$ , with respect to the reference lipid composition  $\mathbf{L}_{\text{exp}}$ , when the parameters of the model are uncertain. This point can be illustrated with the data obtained in the preceding section through our sensitivity analysis. Fig. 6 shows the probability distribution of steady-state compositions  $\mathbf{L}^*$  as a function of  $J_s^{\text{mix}}$  and  $\|\mathbf{L}^* - \mathbf{L}_{\text{exp}}\|_1$ , the distance to the experimental lipid composition, in the absence and in the presence of feedback.

In the absence of feedback (Fig. 6 A), the data show that a majority of  $\mathbf{L}^*$  are close to  $\mathbf{L}_{\text{exp}}$ , but a range of lipid mixtures is allowed by the system. Note that the system does not by default evolve toward pure, monocomponent compositions. In addition, the  $\mathbf{L}^*$  in the biologically viable region ( $J_s^{\text{mix}} > -1/6 \text{ nm}^{-1}$ ) consist mostly of mixtures of PG, DGLcDAG, and GPDGLcDAG, and not of the intermediates PA, CDP-DAG, or PGP. On the other hand, the inviable  $\mathbf{L}^*$ , with  $J_s^{\text{mix}} < -1/6 \text{ nm}^{-1}$ , appear through the increase in MGLcDAG, and not of DAG. These trends stem from the constraints that the network structure imposes on the control mechanism and highlight how the steady-state  $J_s^{\text{mix}}$  is bounded by the simplex of the  $J_s$  values of the individual lipids.

Fig. 6 B shows that the most notable effect of the feedback is to reduce the likelihood of inviable states with values of  $J_s^{\text{mix}} < -1/6 \text{ nm}^{-1}$ , specifically those with high concentrations of MGLcDAG. In addition, our numerical results clearly indicate that the control is not achieved by targeting specific

(possibly monocomponent) compositions, as the overall shape of the probability distribution remains broadly unchanged and mixed states are the norm. In fact, the proportion of monocomponent states is reduced when the feedback is on. Another effect of the feedback is the increase of the probability of states with  $J_s^{\text{mix}}$  close to the boundary between bilayer and nonbilayer states. This follows from the functional form of the feedback that is centered on the value  $c_{\text{bound}}/2 = -1/6.3 \text{ nm}^{-1}$ . This is clearly observable in Fig. 6. The implication is that lipid compositions with large negative  $J_s^{\text{mix}}$  are more improbable, but at the same time there is an increase in lipid compositions with  $J_s^{\text{mix}}$  close to the bilayer to nonbilayer transition.

### The effect of the length of the amphipathic $\alpha$ -helices

As seen in Fig. 3 B, the proposed biophysical feedback exerted by a 19-residue amphipathic  $\alpha$ -helix gives rise to a fourfold regulation, which results in a modest reduction of the likelihood of inviable states. The functional form of our feedback implies that the magnitude of the feedback depends strongly on the length of the amphipathic  $\alpha$ -helix. We now investigate how the length and number of amphipathic  $\alpha$ -helices on MGS and DGS affect  $J_s^{\text{mix}}$  regulation.

Biological evidence indicates that the size of amphipathic motifs should be studied parametrically as it is an important

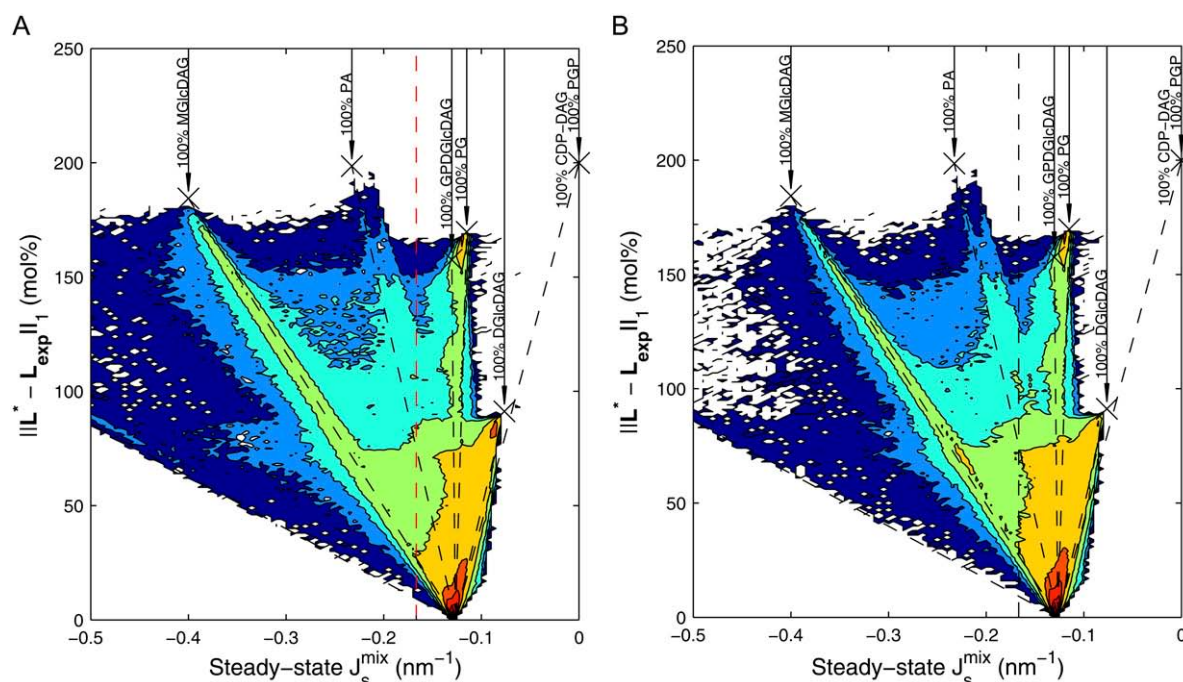


FIGURE 6 Histogram of the distribution of steady-states  $L^*$ , showing the probability distribution of  $J_s^{\text{mix}}$  and the distance of  $L^*$  to the experimental concentration  $L_{\text{exp}}$ . The data are obtained by sampling  $10^6$  random parameter sets as in Fig. 5. (A) Distribution in the absence of feedback. The vertical dashed line at  $J_s^{\text{mix}} = -1/6 \text{ nm}^{-1}$  separates the nonbilayer and bilayer fractions. The dashed lines correspond to the steady-state  $J_s^{\text{mix}}$  that results from adding a particular lipid to  $L_{\text{exp}}$  until one reaches a monocomponent state, marked by crosses. (B) Distribution when both MGS and DGS exert biophysical feedback through a 19-residue amphipathic  $\alpha$ -helix.

feature in protein-membrane interactions. Secondary-structure predictions suggest that both MGS and DGS have multiple  $\alpha$ -helices that may insert into the membrane (20,30). However, it is difficult to identify amphipathic  $\alpha$ -helices and determine their length from genetic sequences. It is also important to mention that some enzymes with amphipathic  $\alpha$ -helices can act in concert. For instance, there is evidence that CCT acts as a dimer that is only active when the 58-residue amphipathic  $\alpha$ -helices of both monomers are bound to the membrane (58). In a simplified picture, this dimer would be viewed as having an effective amphipathic  $\alpha$ -helix of 116 residues.

Fig. 7 plots the dependence on the length of the amphipathic  $\alpha$ -helices of the marginal distribution  $P(J_s^{\text{mix}})$  in Fig. 5 A, where both MGS and DGS are curvature sensitive. Clearly, as the length of the  $\alpha$ -helices is increased, the distribution becomes sharper and the likelihood of getting inviable states is reduced. As the inset of Fig. 7 shows, the reduction in the proportion of nonbilayer states increases to more than 50% when both MGS and DGS have 60-residue  $\alpha$ -helices.

## DISCUSSION

This article outlines a bottom-up modeling framework that couples a biochemical network with an intrinsic biophysical feedback mechanism. The central idea behind the biophysical regulation is that the activity of certain enzymes involved in

lipid biosynthesis is dependent on the spontaneous curvature of the lipids, which is itself a function of the lipid composition. This introduces a feedback loop that can regulate  $J_s^{\text{mix}}$ , a property that must be kept within a narrow window to allow for cellular activity and survival (3,7).

The numerical results of our model show that the system evolves toward biologically plausible mixtures of lipids. When the biophysical regulation is present, it decreases the likelihood of inviable steady-state lipid compositions that would not be expected to form a lamellar bilayer. Moreover, our sensitivity analysis indicates that two enzymes in the network (DGS and MGS) have the largest effect on the steady-state  $J_s^{\text{mix}}$ , in agreement with kinetic data. This fact follows from both the intrinsic properties of the enzymatic reactions (the corresponding substrates have large negative  $J_s$  and the reactions result in large positive changes in  $J_s$ ), and from their position in the lipid biosynthetic network. Therefore, the model underscores the possibility that a chemically nonspecific, biophysical mechanism can participate effectively in the regulation of  $J_s^{\text{mix}}$  in the plasma membrane. Such a mechanism implies that the lipid biosynthetic enzymes regulate the concentration of individual lipids not only as a function of their own concentration but also as a result of larger scale, mechanical properties of the membrane.

The sensitivity analysis used here brings to the fore the importance of characterizing parameter variability in biological systems. Indeed, the sensitivity of  $J_s^{\text{mix}}$  is dependent on

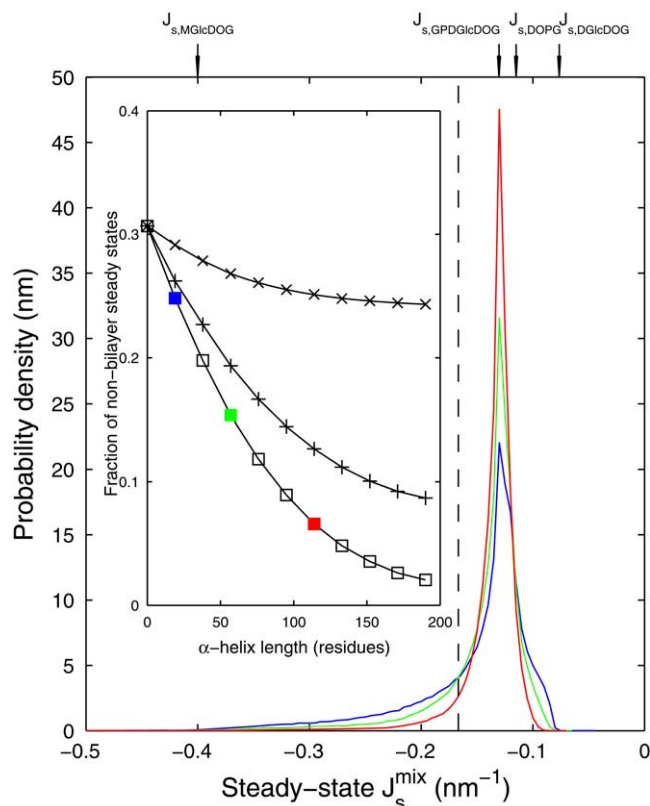


FIGURE 7 Effect of amphipathic  $\alpha$ -helix length on steady-state  $J_s^{\text{mix}}$ . Shown are three marginal distributions  $P(J_s^{\text{mix}})$  of the steady-state  $J_s^{\text{mix}}$  under uncertain parameters where both MGS and DGS are curvature sensitive with amphipathic  $\alpha$ -helices of different lengths: 19-residue (blue, same as Fig. 5 A), 57-residue (green), and 114-residue (red). Vertical dashed line at  $J_s^{\text{mix}} = -1/6 \text{ nm}^{-1}$  indicates the nonbilayer region. (Inset) Probability that the steady state does not form a bilayer against  $\alpha$ -helix length, when MGS has an  $\alpha$ -helix ( $\times$ ); DGS has an  $\alpha$ -helix ( $+$ ); and MGS and DGS both have  $\alpha$ -helices ( $\square$ ). Colored squares correspond to the three plotted  $P(J_s^{\text{mix}})$  in the main figure.

how the parameters are varied. In the absence of additional knowledge, our approach has been to sample the  $V_{\text{cell,Enzyme}}$  parameter sets uniformly according to their relative logarithmic distance to the reference set,  $k$ , with a maximum variation for each individual parameter of  $\sim 2$  orders of magnitude. This leads to mixed steady-state lipid compositions localized mostly in the biologically viable region (Fig. 6). However, if the parameter variation is larger, our numerics indicate that monocomponent steady-state lipid compositions begin to appear. At present, it is difficult to infer from experimental results the range of  $V_{\text{cell,Enzyme}}$  a cell is likely to experience and is likely to be robust to. For example, cells that overexpress enzymes 100 times are often still viable; however, this is unlikely to result in a 100-fold increase in enzyme activity. Clearly, the shape and width of the parameter distributions are an essential part of a meaningful sensitivity analysis of biological systems, and further experimental characterization in this area is needed.

Our study also highlights the importance of the length of the amphipathic  $\alpha$ -helix as it is related (linearly in our simple model) to the energy released when it is inserted into the membrane. This suggests that the membrane binding of short amphipathic  $\alpha$ -helices, such as the eight-residue  $\alpha$ -helix on *E. coli* MinD (46), is less sensitive to  $J_s^{\text{mix}}$ , whereas the binding of long amphipathic  $\alpha$ -helices is much more sensitive to  $J_s^{\text{mix}}$ . In addition, enzymes that act as oligomers provide more effective regulation of  $J_s^{\text{mix}}$ , as seems to be the case with CCT. This aspect of the influence of  $\alpha$ -helix length on the regulation of  $J_s^{\text{mix}}$  could be investigated experimentally by site-directed mutagenesis.

The proposed modeling framework could be extended in several directions. First, our model has been constructed considering amphipathic  $\alpha$ -helices at its core, with an estimate for the binding energy based on a simple geometric calculation of the curvature around an  $\alpha$ -helix. This very simplified picture could be generalized to include entropic contributions and the possibility of more general amphipathic motifs (10). Such an extension would be incorporated into the association constant that encodes the regulation. Second, our model excludes the monoacyl (MA)-derivatives of the glucolipids: MAMGlcDAG, which is rarely present, and MADGlcDAG and MABGPDGlcDAG, which are each only present at  $\sim 10$  mol % when the lipids have a palmitoleoyl fraction  $> 30$  mol % (5). The model could be extended to include the MA-derivatives, although this would require a more detailed understanding of the postulated biosynthetic pathways (59). However, based on the insight provided by the current model, it is unlikely that the enzymes involved in the synthesis of MA-derivatives would have their activity modulated by amphipathic  $\alpha$ -helices, since synthesis of these lipids would lead to a more negative  $J_{s,\text{mix}}$ .

Another extension would be to model the effect of lipid acyl chain length, which directly affects the  $J_s$  of a lipid, on the lipid composition (5,18,60). In its present form, the model only considers lipids with oleoyl acyl chains. However, Fig. 6 illustrates how important the individual lipid spontaneous curvatures are in determining the steady-state  $J_s^{\text{mix}}$ . Experimentally, it is known that if *A. laidlawii* is fed shorter and saturated fatty acids (making the  $J_s$  values in Table 1 more positive), the organism reacts by changing the proportion of lipid headgroups (5). The length and saturation of the lipid acyl chains have a nonlinear, but as yet unquantified, effect on the spontaneous curvature (39). The challenge is to model how the length and degree of unsaturation of the lipid acyl chains affect the lipid  $J_s$  values and to relate this to lipid biosynthesis. Based on our results, the acyl chain length will undoubtedly affect the regulatory role of MGS and DGS. When the lipids have shorter, saturated acyl chains, MGlcDAG and DAG are present at a significantly higher molar fraction. Since MGS catalyzes the reaction between these two lipids, it is hypothesized that when the lipids have shorter, saturated acyl chains, MGS will play a larger regulatory role.



The model can be used to study lipid biosynthesis in other organisms, but it would have to be extended to deal with the particular biochemical and biophysical characteristics of each network. In particular, it is likely that more lipid species will be present, thus increasing the dimensionality of the model and leading to diverse control strategies in different organisms. For instance, *E. coli* is known to regulate  $J_s^{\text{mix}}$  by changing the unsaturation of the lipid acyl chains (7). This results in a combinatorial increase in the number of chemical species and to a lesser extent the number of enzymes. In addition, a detailed understanding of the lipid-dependent activity of the enzymes that control the metabolism of lipid acyl chains would also be necessary. This does, however, highlight the importance of characterizing the biophysical properties of individual lipid types including the values of their monolayer spontaneous curvature. At present this is a relatively neglected area of research and this is a damaging oversight given the role of lipids in regulating key biological processes.

Finally, the connection of lipid biosynthesis to the cell cycle and the spatial inhomogeneity of lipids are two closely interconnected areas in which the modeling framework could be extended. Lipid biosynthesis is linked to the cell cycle by the need to double the lipid mass before cell division (61). Furthermore, experiments show that the anionic lipid cardiolipin (62) and peptides that contain amphipathic  $\alpha$ -helices, such as MinD (63) and MGS (45), localize at the bacterial poles. This localization may act as a trigger for lipid biosynthesis and cell division. Experimental evidence also shows that bacterial membranes may exhibit transbilayer asymmetry (64) and may be divided into domains, for instance a septal and a polar region (62), which have vastly different lipid compositions and enzyme concentrations. In these cases, the modeling framework could be extended to model the lipid compositions in the different lipid domains and lipid monolayers separately.

## APPENDIX A: LIPID COMPOSITIONS AND $J_s$ VALUES (TABLE 1)

The lipid composition in Table 1 is Extract 13 from Andersson et al. (5). This lipid composition also contains 3.2 mol % of the monoacyl-DGlcDAG (MADGlcDAG), which we model as MGlcDAG in Table 1. The assumption is that the  $J_s$  of MADGlcDAG (2 glucose: 3 acyl chains) is close to that of MGlcDAG (1 glucose: 2 acyl chains). The molar fractions of DAG and the lipid intermediates, PA, CDP-DAG, and PGP, are often below the experimental detection limit. In our model, any unaccounted molar fraction is distributed among these lipids and we assume that PA and DAG are present at 20 times the level of CDP-DAG and PGP, based on *E. coli* data (65).

The  $J_s$  values of DOPG (66), dioleoylphosphatidic acid (DOPA) (67), and DOG (39) have been measured experimentally. The  $J_s$  values of DOPG and dioleoylphosphatidic acid are both taken from experiments with a divalent cation concentration above 20 mM. This reproduces the *A. laidlawii* cytoplasmic environment where a divalent cation is bound to 1 in 10 anionic lipids (68). The  $J_s$  values of MGlcDOG, DGlcDOG, and the *A. laidlawii* lipid extracts are estimated from the measured hexagonal phase cylinder diameter  $d$  (18), using the equation  $J_s = 1/(d/2 - 0.9 \text{ nm})$ . CDP-DAG and PGP are

**TABLE 3 Enzyme kinetic constants**

Enzyme	$V_{\text{max}}$ ( $\mu\text{mol mg}^{-1} \text{min}^{-1}$ )	$K_{\text{mL}}$ (molar fraction)	$K_{\text{mS}}$ (mM)	$K_{\text{eqm}}$	Reference
CDP-DAG synthase*	55	†	0.58	0.22	(23)
PGP synthase*	20	†	0.32	N/A	(24)
PA phosphatase	12.8	0.1	N/A	N/A	(27)
MGlcDAG synthase	12	0.08	0.4	N/A	(28)
DGlcDAG synthase	1.3	0.01	0.14	N/A	(29)

\* $V_{\text{max}}$  and  $K_{\text{m}}$  kinetic constants of these enzymes are taken from *E. coli*.

†These enzymes were not studied with the surface dilution mechanism.

present at negligible amounts and their  $J_s$  values are estimated to be  $0 \text{ nm}^{-1}$ . The estimated spontaneous curvature of GPDGlcDOG follows from using the linear assumption in Eq. 2 and the experimental range of lipid extract  $J_s^{\text{mix}}$  values of between  $-1/6.6 \text{ nm}^{-1}$  and  $-1/8.1 \text{ nm}^{-1}$  to give a value of  $J_s = -1/7.7 \text{ nm}^{-1}$ . This estimated value suggests GPDGlcDAG forms a lipid bilayer and is consistent with observations that GPDGlcDAG, with a mixture of palmitoyl and oleoyl acyl chains, forms a mixture of micellar and lamellar aggregates (69). The  $J_s$  value of the anionic lipid GPDGlcDAG is also likely to depend on the concentration of free and bound cations (66). The lipid  $J_s$  values in Table 1 give a  $J_s^{\text{mix}}$  in the experimental range for all other measured oleoyl acyl lipid compositions (5,18).

## APPENDIX B: LITERATURE MODEL PARAMETERS (TABLE 2)

### Functional forms for $V_{\text{GPDGs}}$ and $V_{\text{CDS}}$

Two reactions of the lipid biosynthetic network are not described by Eq. 3, which is an irreversible Michaelis-Menten kinetic rate equation with one lipid substrate and one soluble substrate. GPDGs catalyzes an irreversible reaction, but the reaction involves two lipid substrates. This gives a rate equation with the functional form,

$$v_{\text{Enzyme}} = V_{\text{cell}} \frac{\frac{\{L\}_i \{L\}_j}{K_{\text{mLi}} K_{\text{mLj}}}}{1 + \frac{\{L\}_i}{K_{\text{mLi}}} + \frac{\{L\}_j}{K_{\text{mLj}}}} \quad (\text{B1})$$

The reaction catalyzed by CDS is reversible and is modeled with a reversible rate equation,

$$v_{\text{Enzyme}} = V_{\text{cell}} \frac{\frac{\{L\}_i [S]}{K_{\text{mL}} K_{\text{mS}}} \left( 1 - \frac{\{L\}_j [P]}{\{L\}_j [S]} \right)}{1 + \frac{\{L\}_i}{K_{\text{mL}}} + \frac{[S]}{K_{\text{mS}}} + \frac{\{L\}_j}{K_{\text{mL}}} + \frac{[P]}{K_{\text{mS}}}} \quad (\text{B2})$$

**TABLE 4  $V_{\text{cell}}$**

Enzyme	Enzyme yield	$V_{\text{cell, Enzyme}}$ ( $\text{min}^{-1}$ )	Reference
CDP-DAG synthase	1/8000*	$9.6 \times 10^{-3}$	(23)
PGP synthase	1/6000*	$4.7 \times 10^{-3}$	(24)
PA phosphatase	1/440	$4.1 \times 10^{-2}$	(27)
MGlcDAG synthase	1/9100	$1.8 \times 10^{-3}$	(28)
DGlcDAG synthase	1/5250	$3.5 \times 10^{-4}$	(29)

\*Enzyme yield of these enzymes is taken from *E. coli*.

**TABLE 5 Soluble reactant concentrations**

Reactant	Concentration (mM)	Reference
CTP	0.5	(72)
PP <sub>i</sub>	6*	(73)
G3P	0.2*	(74)
UDP-glucose	0.4*	(75)

\*These intracellular concentrations are not from *A. laidlawii*.

where  $[P]$  is the soluble product bulk concentration; the lipid product and soluble product Michaelis constants are assumed to be equal to the substrate Michaelis constants  $K_{mL}$  and  $K_{mS}$ , respectively; and  $K_{eqm}$  is the equilibrium constant.

## Enzyme kinetic constants

Three of the seven *A. laidlawii* lipid biosynthetic enzymes have been studied in detail. In addition, we use experimental data for two other reactions from *E. coli*. Although *E. coli* and *A. laidlawii* are very different organisms, most sequenced bacterial genomes are found to encode a protein that has a strong homology to CDP-DAG synthase of *E. coli* (22). Table 3 summarizes the corresponding  $V_{max}$ ,  $K_{mL}$ ,  $K_{mS}$ , and  $K_{eqm}$  values.

The  $V_{cell}$  values are obtained from Eq. 4 using the  $V_{max}$  in Table 3 and the ratio  $M_{Enzyme}/N_{Lipid}$  (protein mass to moles of lipid per cell), which is estimated as follows. *A. laidlawii* has 1.35  $\mu\text{mol}$  of polar lipid for each milligram of membrane protein (70). Polar lipids constitute  $\sim 40\%$  of the *A. laidlawii* membrane. Membrane proteins are measured to constitute 21.2% of the overall protein mass (71). This gives an  $M_{Protein}/N_{Lipid}$  ratio of 1.4 mg  $\mu\text{mol}^{-1}$ . The enzyme yield  $M_{Enzyme}/M_{Protein}$  is taken from the purification of each enzyme and is given in Table 4, which also presents the resulting estimate of  $V_{cell}$ .

## Soluble reactant concentrations

The rate equations for the enzymatic reactions feature the soluble substrates G3P and uridine diphosphate (UDP)-glucose, CTP, and PP<sub>i</sub>. In our model, we assume that the soluble metabolites are not dynamic variables and have the constant, regulated cytoplasmic concentrations in Table 5. This assumption is motivated by their involvement in many cellular processes other than lipid biosynthesis.

## Lipid insertion

The enzyme that synthesizes PA in *A. laidlawii* is not well characterized. Therefore,  $V_{+,PA}$  is estimated from the doubling time of *A. laidlawii*. In an exponentially growing membrane, the number of lipids is given by

$$N_{Lipid}(t) = N_{Lipid}(0)\exp(tV_{+,PA}). \quad (\text{B3})$$

Taking the doubling time of *A. laidlawii* in the exponential growth phase to be between 80 and 90 min (Å. Wieslander, University of Stockholm personal communication, 2003, 2004),  $V_{+,PA}$  is  $8.2 \times 10^{-3} \text{ min}^{-1}$ .

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